

## **Fracture behavior of MOD restorations reinforced by various fibre-reinforced techniques – an in vitro study**

Tekla Sary<sup>1</sup>, Sufyan Garoushi<sup>2</sup>, Gabor Braunitzer<sup>3</sup>, David Alleman<sup>4</sup>  
Andras Volom<sup>1</sup>, Mark Frater<sup>1\*</sup>

<sup>1</sup>Department of Operative and Esthetic Dentistry, Faculty of Dentistry,  
University of Szeged, Szeged, Hungary

<sup>2</sup>Department of Biomaterials Science and Turku Clinical Biomaterials Center -  
TCBC, Institute of Dentistry, University of Turku, Turku, Finland

<sup>3</sup>dicomLAB Dental Ltd., Szeged, Hungary

<sup>4</sup>The Alleman Center for Biomimetic Dentistry, Utah, USA

### **Conflicts of Interests**

All authors declare to have no conflict of interests.

\*Corresponding author:

Dr. Mark Frater, DMD, PhD, M.Sc. assistant professor and head of the department  
Department of Operative and Esthetic Dentistry  
Faculty of Dentistry  
University of Szeged  
Tisza Lajos Krt. 64-66.  
H-6720  
Szeged, HUNGARY  
+36303192937

E-mail address: meddentist.fm@gmail.com

## **Abstract:**

**Purpose:** The aim was to evaluate the fracture resistance of various direct restorative techniques utilizing different fibre-reinforced materials for restoring deep class II. MOD cavities in molar teeth.

**Material and Methods:** Two hundred forty intact mandibular third molars were randomly divided into twelve groups (n=20). Except for the control group (G12), deep mesio-occluso-distal (MOD) cavities were prepared all other groups. After adhesive treatment and rebuilding the missing interproximal walls with composite, the specimen were restored with different fibres and a final occlusal layer of composite as follows: composite only (G1), short fibre-reinforced composite (SFRC) (G2), glass fibre net (GFN) on the base of the cavity buccolingually (BL) and SFRC (G3), SFRC and GFN on top of it BL (G4), SFRC and occlusal splinting with GFN (G5), GFN circumferentially and SFRC (G6), polyethylene fibres (PF) on the base of the cavity BL and composite (G7), composite and PF on top of it BL (G8), composite and occlusal splinting with PF (G9), PF circumferentially and composite (G10), transcoronal splinting with PF (G11). Fracture-resistance for the restored teeth were tested using universal-testing machine. Fracture thresholds and fracture patterns were measured and evaluated.

**Results:** The transcoronal splinting (G11) yielded the highest fracture resistance among the restored groups. Groups 1, 3 and 4 showed significantly lower fracture resistance values compared to intact teeth.

**Conclusion:** Incorporating polyethylene or a combination of short and bidirectional glass fibres in certain positions in direct restorations seems to be able to restore the fracture resistance of sound molar teeth.

**Key words:** MOD cavity; short fibre-reinforced composite; glass fibre net; polyethylene; fracture toughness; splinting

## 1. Introduction

Placement and replacement of direct restorations belong to the most frequently performed interventions in general dentistry. Given the high patient demand for tooth-colored restorations that make a natural impression, the use of direct posterior composite resin (CR) restorations has widely increased for such purposes.<sup>1</sup> The number of direct posterior CR restorations will continue to increase with the worldwide phasedown in the use of amalgam.<sup>2-4</sup> In addition to the aesthetic considerations, a restoration must also restore function and preserve the remaining tooth structure against fracture.<sup>5</sup>

This is highly important in case of large carious defects and subsequent cavities (e.g. mesio-occluso-distal (MOD) cavities). Extensive cavity preparation is one of the primary reasons for tooth fragility, resulting in partial or complete fractures of posterior tooth cusps or even root fractures.<sup>6</sup> A standardized MOD cavity preparation in maxillary premolar teeth was shown to result in 63% average loss in relative cuspal stiffness,<sup>7</sup> which is related principally to the loss of marginal ridge integrity.<sup>8,9</sup> This causes a reduction in fracture strength of approximately 54%.<sup>10,11</sup> It has been shown that cuspal deflection increases with increasing cavity dimensions,<sup>12</sup> meaning the larger the restoration's volume, the higher the stress generated in the remaining dental structure. This is in accordance with both in vitro and clinical findings, showing that in general, for both molar and premolar teeth, the higher the number of restored surfaces and the wider the isthmus of the restoration, or both, the greater the chance of cuspal fracture with time.<sup>13</sup> CR restorations have the advantage of bonding to tooth structure, thus theoretically providing an „internal splint”, which might strengthen the tooth and help regain its lost fracture resistance. However, the reinforcing effect of direct composite fillings alone in deep MOD cavities is highly debated. The increased use of composite materials in the posterior region brought about technological advances as new materials were needed to overcome the shortcomings of conventional composite fillings.

The development of fibre-reinforced composite (FRC) technology allowed the use of CR materials in extensive preparations.<sup>14</sup> In 2013, a short fibre-reinforced composite (SFRC) (EverX Posterior; GC, Tokyo, Japan) was introduced as a dental restorative CR intended to be used in high-stress-bearing areas in both vital and non-vital teeth, especially in molars.<sup>15,16</sup> As the fibres incorporated into the SFRC have a length equal to or greater than the critical fibre length (0.5 - 1.6 mm),<sup>17</sup> it is able to act as a stress-absorbing, dentine-replacing material.<sup>15</sup> The randomly oriented fibres in SFRC provide reinforcement in three directions, whereas bidirectional or woven continuous fibres provide reinforcement in only two directions.<sup>18</sup> Theoretically, however, the directional distribution of reinforcement is less effective in SFRC, since a certain volume of fibres is divided in three directions.<sup>19</sup> So far continuous bi-directional FRC (EverStick NET; GC, Tokyo, Japan) has been used to reinforce or repair provisional fixed partial dentures<sup>20</sup> or reinforce indirect composite restorations by being applied in the intaglio<sup>21</sup> or placed under endocrowns,<sup>22</sup> but not for direct restorative purposes inside cavities.

Also, in the past 20 years, a leno woven ultra high molecular weight (LWUHMW) polyethylene fibre ribbon (Ribbon THM; Ribbon Inc., Seattle WA, USA), inserted into a bed of flowable composite, have been used in various direct restorative techniques. The purpose of the polyethylene fibres is manifold: partly to form a stress-absorbing layer and redirect potential cracks and fractures,<sup>23</sup> and partly to internally splint the tooth and increase fracture strength.<sup>14</sup> Application techniques included lining the fibre under the composite filling<sup>14,24,25</sup> or over the finished composite restoration by preparing a groove<sup>25</sup> or applying the fibres inside the axial walls circumferentially.<sup>26</sup>

The question arises whether continuous bidirectional FRC could be used in cavities in the same manner as polyethylene fibres and if they could amplify the reinforcing effect of SFRC.

The purpose of this in vitro investigation was to assess the reinforcing effect of different FRC materials compared to polyethylene ribbon fibres with conventional composite in direct restorative techniques applied in class II deep MOD cavities.

The null hypothesis was that (1) the teeth restored with the tested restorative techniques would show similar mechanical resistance as intact molar teeth, and that (2) the fracture patterns in molar teeth with deep class II cavities would not depend on the applied restorative technique.

## **2. Material and methods**

240 mandibular third molars extracted for periodontal or orthodontic reasons were selected for this study. The freshly extracted teeth were immediately placed in 5.25% NaOCl for 5 minutes and then stored in 0.9% saline solution at room temperature until use all within 2 months of extraction. During specimen preparation, the soft tissue covering the root surface was removed with hand scalers. The inclusion criteria were visual absence of caries or root cracks, absence of previous endodontic treatment, posts or crown or resorptions. Teeth with severe polymorphism of the coronal structures were excluded from the investigation.

About eighty percent of the specimens ranged 10.0 to 10.9 mm in size, measured at the widest bucco-lingual dimension, and the rest were between 11.0 and 12.0 mm. The mesio-distal dimension of the samples was also measured and this parameter allowed a maximum deviation of 10% from the determined mean. The teeth were randomly distributed over 12 study groups (n=20) (see below).

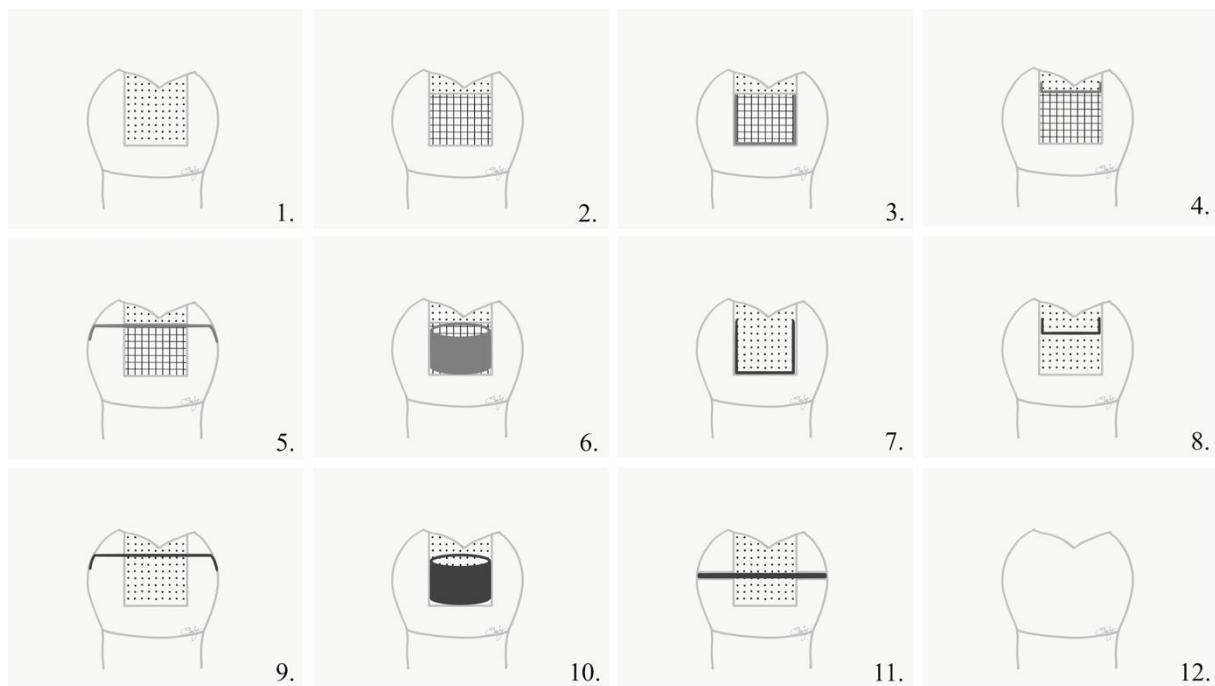
### **2.1. Cavity preparation and restorative procedures**

One group was left intact to serve as a control (Group 12). The rest of the teeth received standardised MOD cavity preparation with 2.5 mm wall thicknesses and with 5 mm depth prepared by the same trained operator as described by Forster et al.<sup>27</sup> The preparation was performed with a round end parallel diamond (881.31.014 FG - Brasseler USA Dental, Savannah, GA) bur initially positioned at the midline of the occlusal surface of the teeth (determined by dividing the distance between the buccal and lingual cusp tips). The thickness of the opposing walls at the cavity base were continuously checked during the preparation with a digital calliper (Mitutoyo Corp., Kawasaki, Japan) and adjusted to have a uniform 2.5 mm thickness at the base of the cavity. The cavity walls were prepared parallel to the axis of the tooth. The depth of the cavity was evaluated with a 15 UNC periodontal probe (Hu-Friedy Mfg. Co., Chicago, USA) measured from the corresponding cusp tip by touching the cavity wall with full length of the instrument. The cavity was one continuous cavity with the proximal box having exactly the same width (2.5 mm) and depth (5 mm) as the occlusal one. The cavosurface margins were prepared perpendicular to the tooth surface at the end of the preparation. Only in

Group 11, on both buccal and lingual walls, an artificial whole with a width of approx. 2-3 mm was prepared on the occlusal third of the wall with a diamond micropreparation bur (MP 53, TwoStriper, Airbrasive Tehcnology inc. USA). After the preparation all cavities were rinsed with water and air-dried with an air/water syringe. The cavities received the same adhesive treatment. After application of a Tofflemire (1101C 0.035, Hawe-Neos, Italy) matrix band, the enamel was acid-etched selectively with 37% phosphoric acid for 15 seconds, rinsed with water and air-dried. The cavity was adhesive-treated with G-Premio Bond (GC Europe, Leuven, Belgium) according to the manufacturer's instructions. The adhesive layer was light-cured for 40 s with an Optilux 501 halogen light (Kerr, Orange, CA, USA) operating in standard mode at a light intensity of 740+/- 36 mWcm<sup>2</sup>. In all groups, an approximately 0.5 mm-thick flow composite layer (G-aenial Flo, GC Europe, Leuven, Belgium) was applied on the floor of the cavity. This layer was light-cured for 40 s. After applying the flowable, the interproximal walls were build-up with composite (G-aenial Posterior PJ-E, GC Europe, Leuven, Belgium) using the centripetal technique, thus transforming the MOD cavity into a class I. cavity.

From this point the cavities were distributed among 11 groups according to the different direct restorative techniques. The cavities were restored as follows (see figure 1.):

**Figure 1.** Schematic figure representing the test groups (Group 1-12).



Group 1: The cavities were restored with micro hybrid composite restorative material (G-aenial Posterior PJ-E, GC Europe, Leuven, Belgium) applied with an oblique incremental technique. The material was placed in consecutive 2 mm thick increments. Each increment was light cured from the occlusal surface for 40 seconds. Glycerine gel (DeOx Gel, Ultradent Products Inc., Orange, CA, USA) was applied and final polymerization from each side for 40 seconds with Optilux 501 was performed. The finishing and polishing was the same in all groups, meaning the restoration was finished with a fine granular diamond burr (FG 7406-018, Jet Diamonds, USA and FG 249-F012, Horico, Germany) and aluminum oxide polishers (OneGloss PS Midi, Shofu Dental GmbH, Ratingen, Germany).

Group 2: The cavities were restored with an SFRC material (EverX Posterior, GC Europe, Leuven, Belgium) applied in a bulk-fill technique. The material was placed in single increment according to the anatomy of the dentine, leaving 1,5-2 mm occlusally for the final composite layers as prescribed by the manufacturer. This increment was light cured from the occlusal surface for 40 seconds. The last occlusal layer was composite material (G-aenial Posterior PJ-E, GC Europe, Leuven, Belgium) covering the SFRC. Glycerine gel (DeOx Gel, Ultradent

Products Inc., Orange, CA, USA) was applied and final polymerization from each side for 40 s with Optilux 501 was performed.

Group 3: A piece of 3 mm wide pre-impregnated glass fibre net (Everstick NET, GC Europe, Leuven, Belgium) with a size approx. the same as the remaining cavity was cut and placed on the cavity walls in a bucco-lingual direction. The net was placed in a way that it would not reach the margins of the cavity, leaving 1,5-2 mm space for the future occlusal composite layer. In all groups where the net was used, it was adapted to the walls with a periodontal probe (Hu-Friedy Mfg. Co., Chicago, USA) slightly wetted in resin (Stick resin, GC Europe, Leuven, Belgium) and handled according to manufacturer's instructions. After curing for 40 s, the cavity was restored with SFRC and a final layer of occlusal composite as in Group 2.

Group 4: The cavities were restored with SFRC as described in Group 2. When there was only approx. 1.5-2 mm space remaining of the cavity occlusally, a piece of 3 mm wide pre-impregnated glass fibre net (Everstick NET, GC Europe, Leuven, Belgium) was placed on the cavity walls in a bucco-lingual direction. The net was placed in a way that it would not reach the margins of the cavity. After curing for 40s, the cavity was restored with a final layer of occlusal composite as in Group 2.

Group 5: The cavities were restored with SFRC and a final layer of occlusal composite as in Group 2. After finishing the restoration, a groove 4 mm wide and 1,5 mm depth was prepared on the occlusal surface of the restorations between the cusp tips, from a buccal to lingual direction, with a high speed bur under water cooling. The ends of the groove were on the occlusal one-third of the buccal and lingual walls of the teeth. After selective enamel etching in the mentioned area, the groove was rinsed, dried and adhesively treated (G-Premio Bond, GC Europe, Leuven, Belgium). A piece of pre-impregnated glass fibre net (Everstick NET, GC Europe, Leuven, Belgium) with a size of the prepared groove was cut and placed into the groove. After curing for 40s, the cavity was restored with a final layer of occlusal composite as in Group 2.

Group 6: 1 piece of 3 mm wide pre-impregnated glass fibre net (Everstick NET, GC Europe, Leuven, Belgium) was placed on the cavity walls circumferentially. The net was placed in a



way that it would cover the axial walls but not reach the margins of the cavity. After curing for 40s, the cavity was restored with SFRC and a final layer of occlusal composite as in Group 2.

Group 7: 1 pieces of 3 mm wide LWUHMW polyethylene ribbon fibres (Ribbond-Ultra THM; Ribbond Inc., Seattle WA, USA) were placed into the cavity covering the cavity walls in a bucco-lingual direction forming a fibre layer with Ribbond just as in group 3 with the glass fibre net. In all groups where polyethylene fibres were used, the fibres were first saturated with adhesive resin (Stick Resin, GC Europe, Leuven, Belgium), the excess adhesive resin was removed with a hand instrument and then placed into the bed of un-cured flowable composite (G-aenial universal flo, GC Europe, Leuven, Belgium). The fibre was placed in a way that it would not reach the margins of the cavity. After curing for 40s, the cavity was restored with microhybrid composite as in Group 1.

Group 8: The cavities were restored with a microhybrid composite applied in an oblique incremental technique. The material was placed in consecutive 2 mm thick increments. Each increment was light cured from the occlusal surface for 40 seconds. When there was only approx. 1.5-2 mm space remaining of the cavity occlusally, 1 piece of 3 mm wide LWUHMW polyethylene ribbon fibres (Ribbond-Ultra THM; Ribbond Inc., Seattle WA, USA) was cut and placed in the remaining cavity in a bucco-lingual direction forming a fibre layer with Ribbond just as in Group 4 with the glass fibre net. After handling of the fibres and curing for 40s, the cavity was restored with a final layer of occlusal composite as in Group 1.

Group 9: the cavity was restored with microhybrid composite as in Group 1. After finishing the restoration, a groove 4-mm wide and 1-mm depth was prepared on the occlusal surface of the restorations between the cusp tips, from a buccal to lingual direction, with a high speed bur under water cooling. The ends of the groove were on the occlusal one-third of the buccal and lingual walls of the teeth. After selective enamel etching in the mentioned area, the groove was rinsed, dried and adhesively treated (G-Premio Bond, GC Europe, Leuven, Belgium). A piece of LWUHMW polyethylene ribbon fibre (Ribbond-Ultra THM; Ribbond Inc., Seattle WA, USA) was placed into the groove. After handling of the fibres and curing for 40s, the cavity was restored with a final layer of occlusal composite.

Group 10: A piece of LWUHMW polyethylene ribbon fibre (Ribbond THM; Ribbond Inc., Seattle WA, USA) was cut and placed on the cavity walls circumferentially. The fibre was handled and adapted into flowable composite as in Group 7. After curing for 40s, the cavity was restored with microhybrid composite as in Group 1.

Group 11: 1 piece of 1 mm wide LWUHMW polyethylene ribbon fibres (Ribbond Ultra Orthodontic; Ribbond Inc., Seattle WA, USA) were placed through the previously performed penetrations on the buccal and lingual walls into the prepared grooves on the external coronal surfaces connecting the opposing walls like a tightrope. First the polyethylene fibres were fixed in one groove, light cured and covered with composite, and subsequently the rest of the fibres on the opposing side were tightly positioned with a tweezer and fixed to the opposing groove by light curing and composite coverage. This produced a “transcoronal splinting” inside the cavity. After curing for 40s, the cavity was restored with microhybrid composite as in Group 1.

## **2.2. Embedding and mechanical testing of specimen**

The restored specimen were stored in physiological saline solution (Isotonic Saline Solution 0.9%; B. Braun, Melsungen, Germany) in an incubator (mco-18aic; Sanyo, Moriguchi, Japan) at 37°C. To simulate the periodontal ligament, the root surface of each tooth was coated with a layer of liquid latex separating material (Rubber-Sep, Kerr, Orange, CA) prior to embedding. Specimens were embedded in methacrylate resin (Technovit 4004, Heraeus-Kulzer) at 2 mm from the cemento-enamel junction (CEJ) to simulate the bone level. After embedding, all specimens were immediately subjected to a fracture resistance test. Teeth were quasi-statically loaded with a crosshead speed of 2 mm/minute parallel to the long axis of the tooth in a universal testing machine (5848 MicroTester1, Instron, Norwood, MA, USA) until they were fractured. A cylindrical steel bar 6 mm in diameter and 10 mm long was used.<sup>28,29</sup> The bar was positioned at the centre of the occlusal surface of the tooth crown between the buccal and oral cusps. A force vs. extension curve was dynamically plotted for each tooth (figure 2). Failure load—defined as the load at which the tooth-restoration complex exhibited the first fracture, resulting in a peak formation on the force versus extension curve—was recorded in Newtons (N). In each case the specific failure load was determined when the force versus extension curve showed an abrupt change in load, indicating a sudden decrease in the specimen’s resistance to

compressive loading. After recording failure load, each specimens were visually examined for the type and location of failure, as well as the direction of failure. According to Scotti and co-workers, distinction was made between restorable or nonrestorable fractures under optical microscope with a two-examiner agreement. A restorable fracture is above the CEJ, meaning that in case of fracture, the tooth can be restored, while a nonrestorable fracture extends below the CEJ and the tooth is likely to be extracted.<sup>30</sup>

### **2.3. Statistical analysis**

Statistical analysis was conducted in SPSS 23.0 (SPSS Inc., Chicago, IL). For the comparisons between the groups, ANOVA with Tukey's HSD post-hoc test was used. The general limit of significance was set at  $\alpha = 0.05$ .

### **3. Results**

Table 1 summarizes the fracture thresholds for the different study groups. The transcoronal splinting (Group 11) yielded the highest fracture resistance among the restored groups, and interestingly, this was even slightly higher than that of the control group (intact teeth). Groups 1, 3 and 4 showed significantly lower fracture resistance values compared to intact teeth, thus the null hypothesis was rejected. The results of the post-hoc pairwise comparisons (Tukey's HSD) are given in Table 2. In terms of the fracture patterns (Table 3), the type of fibres and their position within the restoration influenced the ratio of favourable and unfavourable fractures. SFRC only (Group 2) was characterised by the highest percentage of favourable (i.e. reparable) fractures, while composite alone (Group 1) and transcoronal splinting (Group 11) yielded the lowest ratio. Therefore, the null hypothesis regarding fracture patterns was also rejected.

**Table 1.** Descriptive statistics of the results by group. Groups: 1- composite; 2- SFRC; 3- net B-L at the bottom; 4- net B-L at the top; 5- net occlusal splinting; 6- net circumferential; 7- Ribbond B-L at the bottom; 8- Ribbond B-L at the top; 9- Ribbond occlusal splinting; 10- Ribbond circumferential; 11- Ribbond transcoronal splinting; 12- control

<b>Group</b>	<b>Mean (N)</b>	<b>N</b>	<b>SD</b>
<b>Group 1</b>	1629.45	20	503.11
<b>Group 2</b>	1746.25	20	467.50
<b>Group 3</b>	1122.20	20	440.04
<b>Group 4</b>	1408.65	20	314.59
<b>Group 5</b>	1925.60	20	792.69
<b>Group 6</b>	2067.30	20	535.80
<b>Group 7</b>	1834.40	20	578.56
<b>Group 8</b>	2022.05	20	771.41
<b>Group 9</b>	2129.25	20	629.75
<b>Group 10</b>	1906.95	20	538.09
<b>Group 11</b>	2484.80	20	682.90
<b>Group 12</b>	2266.30	20	601.14

**Table 2.** Significance matrix from the post-hoc pairwise comparisons (Tukey’s HSD). The conventions are the same as in Table 1. Empty cells indicate lack of significance.

	Group 1	Group 2	Group 3	Group 4	Group 5	Group 6	Group 7	Group 8	Group 9	Group 10	Group 11	Group 12
Group 1	-										0.000	0.033
Group 2		-									0.005	
Group 3	0.000	0.041	-		0.001	0.000	0.009	0.000	0.000	0.002	0.000	
Group 4	0.000			-		0.0023		0.049	0.007		0.000	
Group 5			0.001		-							
Group 6			0.000	0.023		-						
Group 7			0.009				-				0.026	
Group 8			0.000	0.049				-				
Group 9			0.000	0.007					-			
Group 10			0.002							-		
Group 11			0.000	0.000			0.026				-	0.000
Group 12	0.033		0.000	0.000							0.005	-

**Table 3.** Fracture patterns by group. Numbers of observations and within-group percentages. The conventions are the same as in Table 1.

	G1	G2	G3	G4	G5	G6	G7	G8	G9	G10	G11	G12
<b>reparable</b>	4 (20%)	16 (80%)	8 (40%)	14 (70%)	13 (65%)	14 (70%)	8 (40%)	10 (50%)	10 (50%)	12 (60%)	4 (20%)	18 (90%)
<b>irreparable</b>	16 (80%)	4 (20%)	12 (60%)	6 (30%)	7 (30%)	6 (30%)	12 (60%)	10 (50%)	10 (50%)	8 (40%)	16 (80%)	2 (10%)

#### 4. Discussion

With recent advances in adhesive technology and the appearance of stronger composite materials, molar teeth with significant damage or carious lesion are routinely treated by extensive MOD cavity filling.<sup>31</sup> In this study, deep MOD cavities were restored with various direct restorative techniques. The dimensions of the MOD cavities used in our study are closest to those of a large direct amalgam replacement, which is also becoming common in daily routine.<sup>32</sup> However, polymerization shrinkage is a serious problem for large direct composite restorations,<sup>33,5</sup> resulting in cuspal strains with subsequent stress or disruption of the bond, microleakage and recurrent caries, or even enamel cracking.<sup>5</sup> To minimize the development of stresses, it is important to use incremental placement techniques, in which the layers are polymerized through the cusps. The other inherent problem of composite materials is their inadequate fracture toughness, which was shown to be significantly lower than that of dentine.<sup>26</sup> Fracture within the body (bulk) and margins of restorations and secondary caries have been mentioned as major problems regarding the failure of posterior composites.<sup>34,35</sup> As modern composite resin materials are rigid, they do not lack strength, but they lack toughness.<sup>26</sup> As described by Lassilla et al., fracture toughness is a mechanical property that describes the resistance of brittle materials to the catastrophic propagation of flaws under an applied load.<sup>34</sup> Thus, it describes damage tolerance of the material and can be considered as a measure of fatigue resistance which predicts structural performance. The problem of lack of toughness is especially well seen in extensive direct restorations, as the volume of the material increases in these cases.<sup>36</sup> As a result of the above-mentioned disadvantages, direct composite fillings might not be the best solution in deep MOD cavities in posterior teeth. In our study, teeth restored with layered composite fillings (Group 1) showed significantly lower fracture resistance than intact teeth (group 12) ( $p=0.033$ ). This is in accordance with the results of Forster et al., showing that molar not root canal treated teeth with deep cavities cannot be successfully reinforced with direct composite fillings.<sup>27</sup> The same was shown by Papadopoulos et al., when they compared the fracture resistance of natural teeth with MOD cavities restored with a bulk-fill composite.

<sup>37</sup> Scholtanus et al. found that premolar teeth with MOD cavities restored with direct composite fillings were significantly weaker than intact teeth. However, in their study one cusp was also replaced by composite material. <sup>38</sup> According to Forster et al., in MOD cavities the depth of the cavity is of critical importance when a direct restorative technique is chosen. <sup>27</sup> Not only is the cantilever effect greater in deep cavities, but also the volume of the restorative material, which highlights the shortcomings of conventional composite materials. In our study, this problem is reflected both in fracture resistance values and the fracture pattern of teeth restored with CR fillings. Regarding fracture pattern, Group 1 was characterised by predominantly unrestorable fractures. Stress-absorption and crack-arresting ability is attributed to the dentine-enamel junction (DEJ) and to the dentine adjacent to this interphase. <sup>39</sup> The more structurally compromised the tooth, the lower the proportion of DEJ and sound dentine is, and the higher the chance for catastrophic failure in the restoration-tooth continuum. A material with high fracture toughness can better resist crack initiation and propagation, thus would be ideal to replace the missing DEJ and/or dentine core. SFRC is intended to be used in high-stress-bearing areas and/or in structurally compromised teeth as a dentine replacing material. <sup>40</sup> Mechanical testing has shown major improvements in load-bearing capacity, flexural strength and also the fracture toughness of SFRC in comparison with conventional composite resin materials. Bijelic-Donova et al. showed that SFRC had a statistically higher fracture toughness (2.4 MPa m<sup>1/2</sup>) and fatigue limit than conventional CR resins (range: 0.9-1.1 MPa m<sup>1/2</sup>). <sup>41</sup> They managed to show a strong correlation between fracture toughness and fatigue performance, with SFRC being able to sustain both compressive static and fatigue load. The toughening ability of SFRC over conventional composites is attributed to two main factors: the millimeter-scale short fibres and the unique semi-IPN structure. In our study, teeth restored with SFRC (Group 2) did not show statistically significant difference from intact teeth (Group 12) in terms of fracture resistance. Also, the fracture pattern changed to predominantly favourable fractures, compared to the composite group (Group 1). In fact, the SFRC group produced the highest amount of favourable fractures among the restored groups. This is in accordance with Frater et al. where SFRC was able to shift the fracture pattern to predominantly favourable even in shallower MOD cavities. <sup>42</sup> Several studies have shown that the SFRC substructure supports the composite restoration and serves as a crack-prevention layer. <sup>43-45</sup> The thickness of the SFRC core has

utmost importance, as it influences the failure mode and the crack-arresting mechanism.<sup>15</sup> In this study, SFRC was applied in a biomimetic way, substituting the missing dentine and ending at the level of the lost DEJ, in order to substitute both tissues simultaneously, following Monaco et al., who suggested that the highest fracture resistance could be achieved this way.<sup>46</sup>

Deep MOD cavities are susceptible to fracture,<sup>10</sup> which is mainly caused by the increased cavity dimensions and the loss of marginal ridges,<sup>7</sup> leading to increased cuspal flexure and overall weakening of the tooth.<sup>12</sup> In order to stabilize the remaining opposing cavity walls, several direct methods utilizing fibres as internal connecting or splinting elements have been put forward. So far, reinforcement with fibres has been shown to enhance strength only in a narrow range of dental materials, such as composite resins.<sup>47</sup> In our study, two different materials, namely polyethylene fibre sheet (Ribbond THM; Ribbond Inc., Seattle WA, USA) and a fibre glass net (Everstick NET, GC Europe, Leuven, Belgium) were used in different positions inside the cavity with the aim of stabilizing the opposing walls and reinforcing the tooth structure. Polyethylene fibres possess a dense concentration of fixed nodal intersections that assist in maintaining the integrity of the fabric. This enables the stresses in the bulk of the material to be transferred more effectively because of the well-defined load paths from one area to another.<sup>48</sup> As shown by Eskitascioglu et al., using polyethylene fibre ribbon in combination with bonding agent and flowable composite under composite restoration may act as a stress-absorber due to its lower elastic modulus.<sup>49</sup> In our study, the efficacy of polyethylene fibres in in most groups did not depend on their position within the direct restoration as there was no statistically significant difference among their fracture resistance values. This is in accordance with Akman et al. who did not find significant difference when restoring root canal treated teeth with MOD cavities using polyethylene fibres in different configurations and positions.<sup>48</sup> In our study, the only exception was between Group 7 and Group 11 ( $p=0.026$ ) among the groups with polyethylene fibres. The use of these fibres seems to be beneficial since groups with polyethylene fibres did not differ significantly from the intact teeth, whereas teeth restored with composite alone showed significantly weaker fracture resistance compared to intact teeth ( $p=0.033$ ). This is contrast to the findings of Belli et al..<sup>14,25</sup> However, it must be considered that they tested the polyethylene fibres in root canal treated teeth.



It was shown by Garoushi et al. that the addition of continuous bidirectional or short random FRC substructure under composite resin, the load-bearing capacity of the restorations could be increased.<sup>50</sup> Bidirectional fibres within the fibre glass net give orthotropic properties to the material.<sup>18</sup> Turkaslan et al. found that pre-impregnated bidirectional FRC can reinforce the tooth interface in two directions, distributing the stresses more evenly and increasing the toughness of the restoration by preventing crack propagation.<sup>51</sup> So far EverStick NET has only been used beneath endocrowns and anterior veneers, but not in posterior cavities. Contrary to polyethylene fibres, the reinforcing efficacy of bidirectional fibre glass net does seem to vary with its position within the restoration. Group 3 showed significantly reduced fracture resistance compared to Group 5 ( $p=0.001$ ) and Group 6 ( $p=0.000$ ), while Group 4 was significantly weaker than Group 6 ( $p=0.023$ ). While using polyethylene fibres was beneficial in all groups, fibre glass net could efficiently reinforce teeth only in Groups 5 and 6 (no significant difference from control). Interestingly, in specific positions, namely when applied bucco-lingually on the base of the cavity (Groups 3 and 7) or bucco-lingually in the coronal third of the restoration (Groups 4 and 8), the two different bidirectional materials yielded different reinforcement. Groups 3 and 4 were significantly weaker than Group 7 ( $p=0.009$ ) and Group 8 ( $p=0.049$ ), respectively. This could be attributed to the difference in the quality and quantity of fibres. Of all restored groups, Group 3 was characterised by the poorest results. This is in line with the findings of Oskoe et al..<sup>47</sup> Also, Group 7 (polyethylene fibres laid down on the base of the cavity, connecting the opposing walls) was found to be the weakest among the polyethylene fibre groups. The reason behind this could be that although the opposing walls are connected but the fibres are not stretched and not under tension at all. Previous studies have pointed out that the placement of fibres at the tensile side of CR specimens improves flexure properties.<sup>52,53</sup>

According to the results of Oskoe et al., placing a glass fibre net as occlusal splinting in the occlusal third of the MOD cavities between composite layers significantly increases fracture resistance.<sup>47</sup> In groups having occlusal splinting the extension of the fibre ends through the occlusal one-third of the buccal or lingual walls allowing the fibre to keep the cusps together, as described by Oskolee et al.<sup>47</sup> and Akman et al..<sup>48</sup>

In our study, regardless of which fibre type was used, fibres applied as occlusal splinting resulted in increased fracture resistance and did not differ significantly from intact teeth. This

is only partly in accordance with Belli et al. who managed to show increased fracture resistance with occlusally splinted groups with polyethylene fibres. Still, their restored specimens were significantly weaker than intact teeth.<sup>25</sup> With occlusal splinting, fibres are placed close to the point where force is exerted, which leads to a shorter working arm according to the principles of levers. In addition, placing fibres on the occlusal surfaces keeps buccal and lingual cusps together, leading to higher fracture resistance.<sup>47</sup> Connecting the remaining opposing cavity walls can be also accomplished circumferentially covering the rebuilt mesial and/or distal walls, a technique called “wallpapering” by Deliperi and colleagues.<sup>26</sup> So far, to use of FRC materials to circumferentially connect the walls of MOD cavities was only attempted by Daher et al.,<sup>54</sup> but they performed this externally, around the coronal part of the teeth. In our study, when applied circumferentially, there was no difference between the fibre glass net and polyethylene fibres. Intriguingly, the net applied circumferentially (Group 6) yielded significantly higher fracture resistance than fibre glass net at the base of the cavity (Group 3,  $p=0.000$ ) or in the occlusal third inside the filling (Group 4,  $p=0.023$ ). At the same time, there was no statistically significant difference between the corresponding Ribbond groups (between Group 7,8,9 and 10). Also, it is worth mentioning that fibre glass net together with SFRC in occlusal splinting (Group 5) or circumferentially (Group 6) was not significantly better than SFRC alone (Group 2) in terms of reinforcement. We assume that even when SFRC is used alone as a dentine substitution, the randomly oriented fibres lend an isotropic reinforcement effect in multiple directions instead of in only a few specific directions.<sup>55</sup> Also, the adaptation of SFRC alone could be better to the cavity walls. From a clinical point of view it is worth mentioning that the usage of SFRC alone in a bulk manner was easier and less time consuming compared to using the fibre net or the polyethylene one.

Among all restored groups the transcoronal splinting with polyethylene fibres (Group 11) produced the highest fracture resistance, even slightly exceeding the values of intact teeth. In our opinion, this can be attributed to the fact that the polyethylene fibres are not laid down, like in the other groups, but rather stretched, and put under tension. A similar concept was shown by Karzoun et al. with a FRC post penetrating through the opposing walls.<sup>56</sup> As the polyethylene fibres are positioned to the occlusal third of the crown, it should theoretically hold all benefits as the occlusal splinting group, namely working as an early stress-redirecting layer and producing a shorter working arm under loading. Also, the concept is considered to be

correct biomechanically as polyethylene fibres, due to their inherent dense network of locked nodal intersections, could also serve as a potential crack stopping mechanism, therefore could attempt to act as a potential DEJ substituting layer.

Regarding fracture pattern, in most cases when fibres were incorporated into the direct restoration, the failure was dominantly a favourable one (above the CEJ). The highest ratio of favourable fractures was seen with SFRC alone (Group 2), whereas composite alone (Group 1) and transcoronal splinting (Group 11) yielded the highest ratio of unfavourable fractures. This, again, points to the increasingly recognized problem of large direct composite restorations, that is, that their fracture toughness is suboptimal, and they cannot serve as a good substitute for DEJ. This way, cracks and fractures propagate freely in them, which, ultimately, results in non-restorable damage.

The limitations of this investigation is that static load to fracture test was used to determine maximal fracture resistance instead of applying cyclic loading. According to Taha et al, "In experimental studies, fracture resistance to static loading has been used as a measure of the effect of cavity preparation and/or restoration on tooth strength. Although the fracture load is typically much higher than functional occlusal loads, it is still a valid method for comparing restorative materials and different cavity designs."<sup>5</sup> Also, as stated by Le Bell-Ronnlof et al., static loading is usually the first step in the evaluation process of a novel dental materials and related techniques and is commonly used in order to obtain basic knowledge regarding the fracture behaviour and load capacity of a post restored tooth.<sup>57</sup> Given the mentioned shortcomings, the proposed techniques should require future testing with cyclic dynamic loading.

## 5. Conclusions:

1. Deep MOD cavities in non- root canal treated molars can be reinforced with fibres utilized in direct restorative techniques.
2. The use of polyethylene fibres seems to be always beneficial, regardless of position within the cavity or the restoration.
3. The efficacy of glass fibre net together with SFRC, regarding fracture resistance, is highly dependent on their position within the cavity or in the restoration.

"This is an electronic reprint of the original article. This reprint may differ from the original in pagination and typographic detail. Please cite the original version: [Tekla Sary, Sufyan Garoushi, Gabor Braunitzer, David Alleman, Andras Volom, Mark Frater, Fracture behaviour of MOD restorations reinforced by various fibre-reinforced techniques – An in vitro study, Journal of the Mechanical Behavior of Biomedical Materials, Volume 98, October 2019, Pages 348-356, DOI: <https://doi.org/10.1016/j.jmbbm.2019.07.006> ©2019 Elsevier Ltd. All rights reserved. This manuscript version is made available under the CC-BY-NC-ND 4.0 license. To view a copy of this license, visit <https://creativecommons.org/licenses/by-nc-nd/4.0>. "

4. Bulk-applied SFRC (to substitute dentine and the DEJ) covered with composite can reinforce deep MOD cavities in non- root canal treated molars.
5. If fracture happens with direct composite restorations in deep MOD cavities in non- root canal treated molars, it is predominantly an unfavourable (irreparable) fracture.

### **Acknowledgments**

This study was supported by the UNKP-18-3 New National Excellence Program of The Ministry of Human Capacities.

## References:

1. Behery H, El-Mowafy O, El-Badrawy W, Saleh B, Nabih S (2016) Cuspal Deflection of Premolars Restored with Bulk-Fill Composite Resins. *J Esthet Restor Dent*. Mar-Apr;28(2):122-30. doi: 10.1111/jerd.12188.
2. Astvaldsdottir , Dagerhamn J, van Dijken JW, Naimi-Akbar A, Sandborgh-Englund G, Traneus S, Nilsson M. Longevity of posterior resin composite restorations in adults – A systematic review. *J Dent*. 2015 Aug;43(8):934-54. doi: 10.1016/j.jdent.2015.05.001.
3. Kielbassa AM, Lynch CD, Wilson NH. Editorial: the Minamata convention: the beginning of the (amalgam-free) future? *Quintessence Int*. 2014 Jul-Aug;45(7):547-8. doi: 10.3290/j.qi.a32032.
- 4 FDI World Dental Federation. FDI policy statement on dental amalgam and the Minamata Convention on Mercury: adopted by the FDI General Assembly: 13 September 2014, New Delhi, India. *Int Dent J*. 2014 Dec;64(6):295-6. doi: 10.1111/idj.12151.
5. Taha NA, Palamara JE, Messer HH. Fracture strength and fracture patterns of root filled teeth restored with direct resin restorations. *J Dent*. 2011 Aug;39(8):527-35. doi: 10.1016/j.jdent.2011.05.003.
6. Soares PV, Santos-Filho PC, Martins LR, Soares CJ. Influence of restorative technique on the biomechanical behavior of endodontically treated maxillary premolars. Part I: fracture resistance and fracture mode. *J Prosthet Dent*. 2008 Jan;99(1):30-7. doi: 10.1016/S0022-3913(08)60006-2.

7. El-Helali R, Dowling AH, McGinley EL, et al: Influence of resin-based composite restoration technique and endodontic access on cuspal deflection and cervical microleakage scores. *J Dent* 2013;41:216-222 doi: 10.1016/j.jdent.2012.11.002.
8. Reeh ES, Douglas WH, Messer HH: Stiffness of endodontically-treated teeth related to restoration technique. *J Dent Res* 1989;68:1540-1544 PubMed PMID: 2584522.
9. Wu Y, Cathro P, Marino V. Fracture resistance and pattern of the upper premolars with obturated canals and restored endodontic occlusal access cavities. *J Biomed Res.* 2010 Nov;24(6):474-8. doi: 10.1016/S1674-8301(10)60063-2.
10. Hannig C, Westphal C, Becker K, et al: Fracture resistance of endodontically treated maxillary premolars restored with CAD/CAM ceramic inlays. *J Prosthet Dent* 2005;94:342-349 PubMed PMID: 16198171.
11. Seo DG, Yi YA, Shin SJ, et al: Analysis of factors associated with cracked teeth. *J Endod* 2012;38:288-292 doi: 10.1016/j.joen.2011.11.017.
12. Taha NA, Palamara JE, Messer HH. Cuspal deflection, strain and microleakage of endodontically treated premolar teeth restored with direct resin composites. *J Dent.* 2009 Sep;37(9):724-30. doi: 10.1016/j.jdent.2009.05.027.
13. de V Habekost L, Camacho GB, Azevedo EC, Demarco FF. Fracture resistance of thermal cycled and endodontically treated premolars with adhesive restorations. *J Prosthet Dent.* 2007 Sep;98(3):186-92. PubMed PMID: 17854619.
14. Belli S, Erdemir A, Ozcopur M, Eskitascioglu G. The effect of fibre insertion on fracture resistance of root filled molar teeth with MOD preparations restored with composite. *Int Endod J.* 2005 Feb;38(2):73-80. PubMed PMID: 15667628.
15. Garoushi S, Gargoum A, Vallittu PK, Lassila L. Short fiber-reinforced composite restorations: A review of the current literature. *J Investig Clin Dent.* 2018 Aug;9(3):e12330. doi: 10.1111/jicd.12330.
16. Garoushi S, Mangoush E, Vallittu M, Lassila L. Short fiber reinforced composite: a new alternative for direct onlay restorations. *Open Dent J.* 2013 Dec 30;7:181-5. doi: 10.2174/1874210601307010181.
17. Vallittu PK. High-aspect ratio fillers: Fiber-reinforced composites and their anisotropic properties. *Dent Mater.* 2015;31:1-7. doi:10.1016/j.dental.2014.07.009.
18. Bařaran EG, Ayna E, Vallittu PK, Lassila LV. Load bearing capacity of fiber-reinforced and unreinforced composite resin CAD/CAM-fabricated fixed dental prostheses. *J Prosthet Dent.* 2013 Feb;109(2):88-94. doi:10.1016/S0022-3913(13)60022-0.

19. Dyer SR, Lassila LV, Jokinen M, Vallittu PK. Effect of fiber position and orientation on fracture load of fiber-reinforced composite. *Dent Mater.* 2004 Dec;20(10):947-55. PubMed PMID: 15501323.
20. Vallittu PK. The effect of glass fiber reinforcement on the fracture resistance of a provisional fixed partial denture. *J Prosthet Dent.* 1998 Feb;79(2):125-30. PubMed PMID: 9513095.
21. Vallittu PK. Use of woven glass fibres to reinforce a composite veneer. A fracture resistance and acoustic emission study. *J Oral Rehabil.* 2002 May;29(5):423-9. PubMed PMID: 12028488.
22. Rocca GT, Saratti CM, Poncet A, Feilzer AJ, Krejci I. The influence of FRCs reinforcement on marginal adaptation of CAD/CAM composite resin endocrowns after simulated fatigue loading. *Odontology.* 2016 May;104(2):220-32. doi: 10.1007/s10266-015-0202-9.
23. Rudo DN, Karbhari VM. Physical behaviors of fiber reinforcement as applied to tooth stabilization. *Dent Clin North Am.* 1999 Jan;43(1):7-35, v. PubMed PMID: 9929797.
24. Belli S, Donmez N, Eskitascioglu G. The effect of c-factor and flowable resin or fiber use at the interface on microtensile bond strength to dentin. *J Adhes Dent.* 2006 Aug;8(4):247-53. PubMed PMID: 16958290.
25. Belli S, Erdemir A, Yildirim C. Reinforcement effect of polyethylene fibre in root-filled teeth: comparison of two restoration techniques. *Int Endod J.* 2006 Feb;39(2):136-42. PubMed PMID: 16454794.
26. Deliperi S, Alleman D, Rudo D. Stress-reduced Direct Composites for the Restoration of Structurally Compromised Teeth: Fiber Design According to the "Wallpapering" Technique. *Oper Dent.* 2017 May/Jun;42(3):233-243. doi: 10.2341/15-289-T.
27. Forster A, Braunitzer G, Toth M, Szabo BP, Frater M. In Vitro Fracture Resistance of Adhesively Restored Molar Teeth with Different MOD Cavity Dimensions. *J Prosthodont.* 2019 Jan;28(1):e325-e331. doi: 10.1111/jopr.12777.
28. Soares, C. J. , L. R. Martins , J. M. Pfeifer , and M. Giannini . 2004. Fracture resistance of teeth restored with indirect-composite and ceramic inlay systems. *Quintessence International* 35 4:281–286. PubMed PMID: 15119713.
29. Cobankara FK, Unlu N, Cetin AR, Ozkan HB. The effect of different restoration techniques on the fracture resistance of endodontically-treated molars. *Oper Dent.* 2008 Sep-Oct;33(5):526-33. doi: 10.2341/07-132.
30. Scotti N, Coero Borga FA, Alovisi M, et al. Is fracture resistance of endodontically treated mandibular molars restored with indirect onlay composite restorations influenced by fiber post insertion? *J Dent.* 2012;40:814–820. doi: 10.1016/j.jdent.2012.06.005.

31. Chai H, Lawn BR. Fracture resistance of molar teeth with mesial-occlusal-distal (MOD) restorations. *Dent Mater*. 2017 Jul;33(7):e283-e289. doi: 10.1016/j.dental.2017.04.019.
32. Cara RR, Fleming GJ, Palin WM, Walmsley AD, Burke FJ. Cuspal deflection and microleakage in premolar teeth restored with resin-based composites with and without an intermediary flowable layer. *J Dent*. 2007 Jun;35(6):482-9. Epub 2007 Feb 23. PubMed PMID: 17321029.
33. Plotino G, Buono L, Grande NM, Lamorgese V, Somma F. Fracture resistance of endodontically treated molars restored with extensive composite resin restorations. *J Prosthet Dent*. 2008 Mar;99(3):225-32. doi:10.1016/S0022-3913(08)60047-5.
34. Lassila L, Keulemans F, Sailyoja E, Vallittu PK, Garoushi S. Mechanical properties and fracture behavior of flowable fiber reinforced composite restorations. *Dent Mater*. 2018 Apr;34(4):598-606. doi:10.1016/j.dental.2018.01.002.
35. Demarco FF, Correa MB, Cenci MS, Moraes RR, Opdam NJ. Longevity of posterior composite restorations: not only a matter of materials. *Dent Mater*. 2012 Jan;28(1):87-101. doi: 10.1016/j.dental.2011.09.003.
36. Braga RR, Boaro LC, Kuroe T, Azevedo CL, Singer JM. Influence of cavity dimensions and their derivatives (volume and 'C' factor) on shrinkage stress development and microleakage of composite restorations. *Dent Mater*. 2006 Sep;22(9):818-23. Epub 2005 Dec 20. PubMed PMID: 16368130.
37. Papadopoulos C, Dionysopoulos D, Tolidis K, Kouros P, Koliniotou-Koumpia E, Tsitrou EA. Structural Integrity Evaluation of Large MOD Restorations Fabricated With a Bulk-Fill and a CAD/CAM Resin Composite Material. *Oper Dent*. 2018 Nov 16. doi: 10.2341/18-013-L.
38. Scholtanus JD, Ozcan M. Clinical longevity of extensive direct composite restorations in amalgam replacement: up to 3.5 years follow-up. *J Dent*. 2014 Nov;42(11):1404-10. doi: 10.1016/j.jdent.2014.06.008.
39. Lee JJ, Kwon JY, Chai H, Lucas PW, Thompson VP, Lawn BR. Fracture modes in human teeth. *J Dent Res*. 2009 Mar;88(3):224-8. doi: 10.1177/0022034508330055.
40. Garoushi S, Sailyoja E, Vallittu PK, Lassila L. Physical properties and depth of cure of a new short fiber reinforced composite. *Dent Mater*. 2013 Aug;29(8):835-41. doi: 10.1016/j.dental.2013.04.016.
41. Bijelic-Donova J, Garoushi S, Vallittu PK, Lassila LV. Mechanical properties, fracture resistance, and fatigue limits of short fiber reinforced dental composite resin. *J Prosthet Dent*. 2016b;115:95-102. doi:10.1016/j.prosdent.2015.07.012.
42. Frater M, Forster A, Kereszturi M, Braunitzer G, Nagy K. In vitro fracture resistance of molar teeth restored with a short fibre-reinforced composite material. *J Dent*. 2014 Sep;42(9):1143-50. doi: 10.1016/j.jdent.2014.05.004.



43. Garoushi S, Lassila LVJ, Tezvergil A, Vallittu PK. Static and fatigue compression test for particulate filler composite resin with fiber-reinforced composite substructure. *Dent Mater* 2007e;23:17-23. Epub 2006 Jan 18. PubMed PMID: 16414110.
44. Garoushi S, Vallittu PK, Lassila L. Direct restoration of severely damaged incisors using short fiber-reinforced composite resin. *J Dent* 2007 g;35:731-736. Epub 2007 Jul 5. PubMed PMID: 17614187.
45. Garoushi SK, Lassila LV, Vallittu PK. Fiber-reinforced composite substructure: Load-bearing capacity of an onlay restoration. *Acta Odontol Scand*. 2006a;64:281-285. PubMed PMID: 16945893.
46. Monaco C, Bortolotto T, Arena A, Krejci I. Restoring Nonvital Premolars with Composite Resin Onlays: Effect of Different Fiber-reinforced Composite Layers on Marginal Adaptation and Fracture Load. *J Adhes Dent*. 2015 Dec;17(6):567-74. doi: 10.3290/j.jad.a35251.
47. Oskoe PA, Ajami AA, Navimipour EJ, Oskoe SS, Sadjadi J. The effect of three composite fiber insertion techniques on fracture resistance of root-filled teeth. *J Endod*. 2009 Mar;35(3):413-6. doi: 10.1016/j.joen.2008.11.027.
48. Akman S, Akman M, Eskitascioglu G, Belli S. Influence of several fibre-reinforced composite restoration techniques on cusp movement and fracture strength of molar teeth. *Int Endod J*. 2011 May;44(5):407-15. doi: 10.1111/j.1365-2591.2010.01843.x.
49. Eskitařiođlu G, Belli S, Kalkan M. Evaluation of two post core systems using two different methods (fracture strength test and a finite elemental stress analysis). *J Endod*. 2002 Sep;28(9):629-33. PubMed PMID: 12236304.
50. Garoushi S, Lassila LV, Tezvergil A, Vallittu PK. Load bearing capacity of fibre-reinforced and particulate filler composite resin combination. *J Dent*. 2006 Mar;34(3):179-84. Epub 2005 Sep 8. PubMed PMID: 16150524.
51. Turkaslan S, Tezvergil-Mutluay A, Bagis B, Vallittu PK, Lassila LV. Effect of fiber-reinforced composites on the failure load and failure mode of composite veneers. *Dent Mater J* 2009;28:530-6. PubMed PMID: 19822982.
52. Dyer SR, Lassila LV, Jokinen M, Vallittu PK. Effect of fiber position and orientation on fracture load of fiber-reinforced composite. *Dent Mater*. 2004 Dec;20(10):947-55. PubMed PMID: 15501323.
53. Ellakwa AE, Shortall AC, Shehata MK, Marquis PM. The influence of fibre placement and position on the efficiency of reinforcement of fibre reinforced composite bridgework. *J Oral Rehabil*. 2001 Aug;28(8):785-91. PubMed PMID: 11556961.
54. Daher R, Feilzer AJ, Krejci I. Novel non-invasive reinforcement of MOD cavities on endodontically treated teeth. *J Dent*. 2016 Nov;54:77-85. doi: 10.1016/j.jdent.2016.09.008.

"This is an electronic reprint of the original article. This reprint may differ from the original in pagination and typographic detail. Please cite the original version: [Tekla Sary, Sufyan Garoushi, Gabor Braunitzer, David Alleman, Andras Volom, Mark Frater, Fracture behaviour of MOD restorations reinforced by various fibre-reinforced techniques – An in vitro study, Journal of the Mechanical Behavior of Biomedical Materials, Volume 98, October 2019, Pages 348-356, DOI: <https://doi.org/10.1016/j.jmbbm.2019.07.006> ©2019 Elsevier Ltd. All rights reserved. This manuscript version is made available under the CC-BY-NC-ND 4.0 license. To view a copy of this license, visit <https://creativecommons.org/licenses/by-nc-nd/4.0>. "

55. Garoushi S, Vallittu PK, Lassila LV. Fracture resistance of short, randomly oriented, glass fiber-reinforced composite premolar crowns. *Acta Biomater.* 2007 Sep;3(5):779-84. Epub 2007 Apr 8. PubMed PMID: 17420162.

56. Karzoun W, Abdulkarim A, Samran A, Kern M. Fracture strength of endodontically treated maxillary premolars supported by a horizontal glass fiber post: an in vitro study. *J Endod.* 2015 Jun;41(6):907-12. doi: 10.1016/j.joen.2015.01.022.

57. Le Bell-Rönnlöf AM, Lassila LV, Kangasniemi I, Vallittu PK. Load-bearing capacity of human incisor restored with various fiber-reinforced composite posts. *Dent Mater.* 2011 Jun;27(6):e107-15 doi: 10.1016/j.dental.2011.02.009.